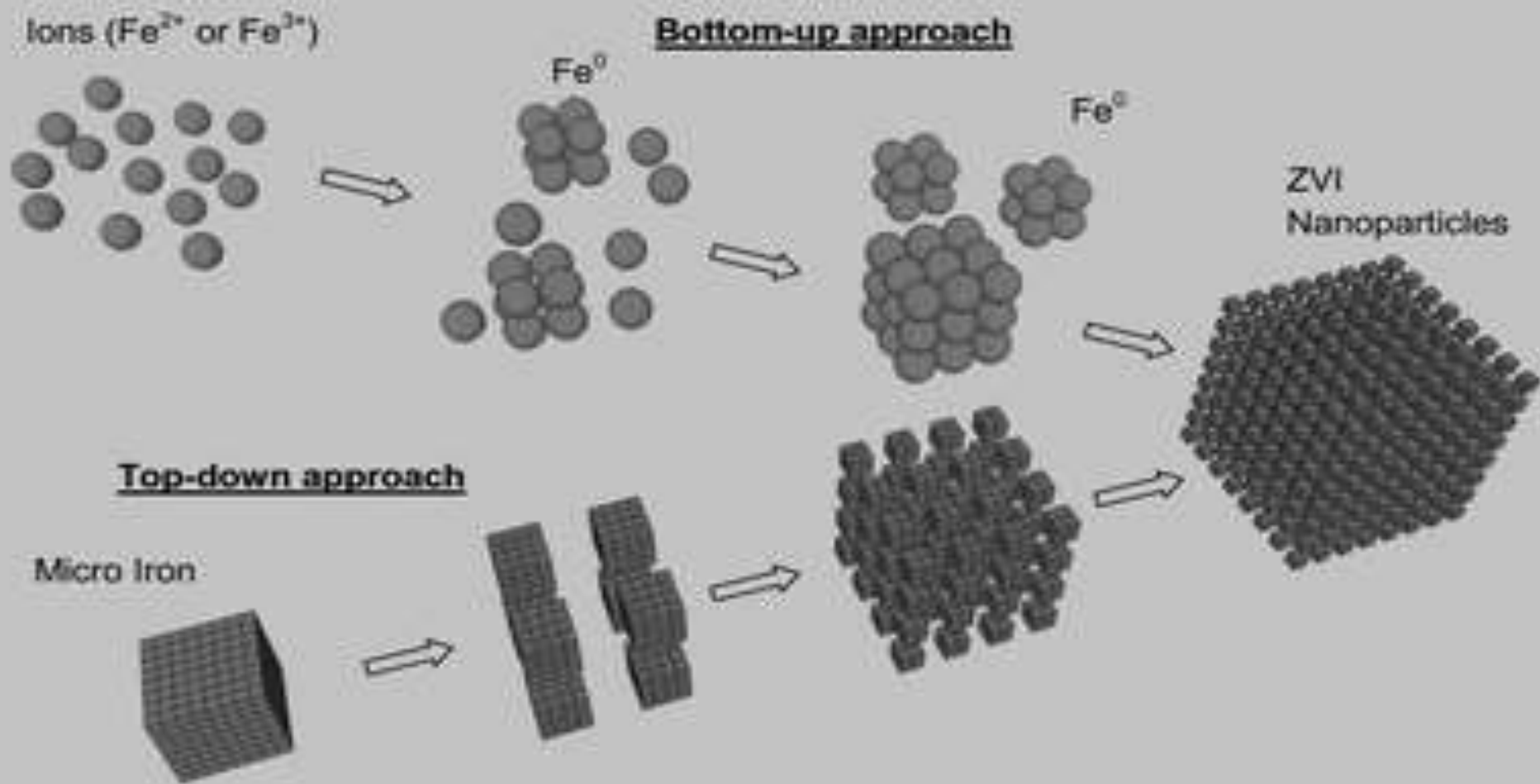


Magnetic nanoparticles for drug delivery

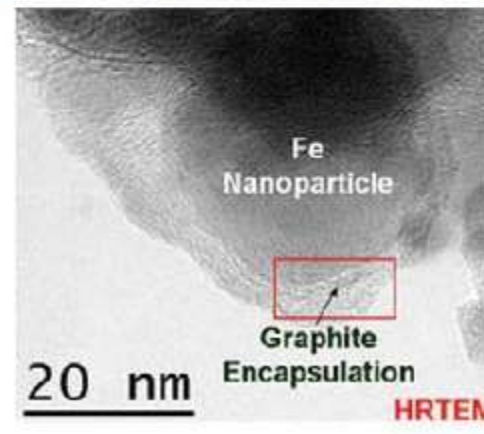
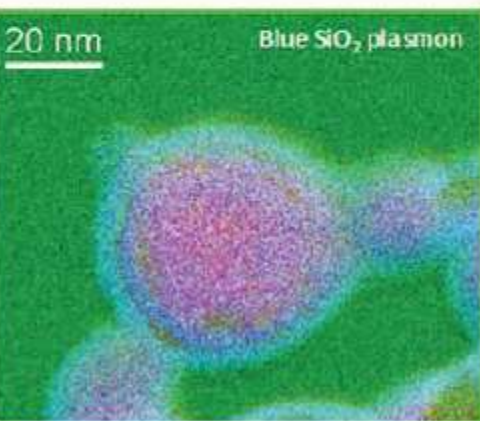
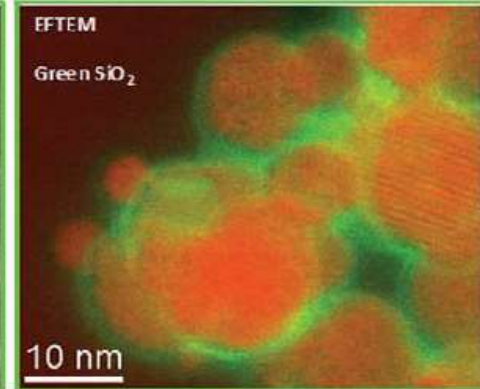
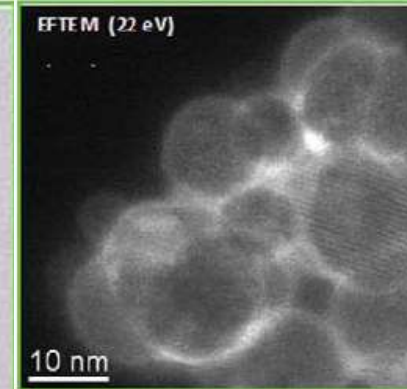
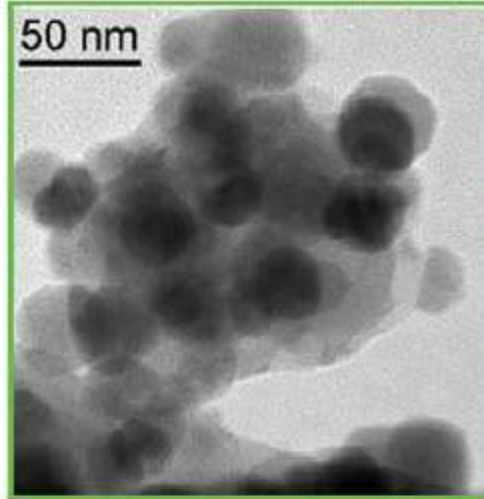
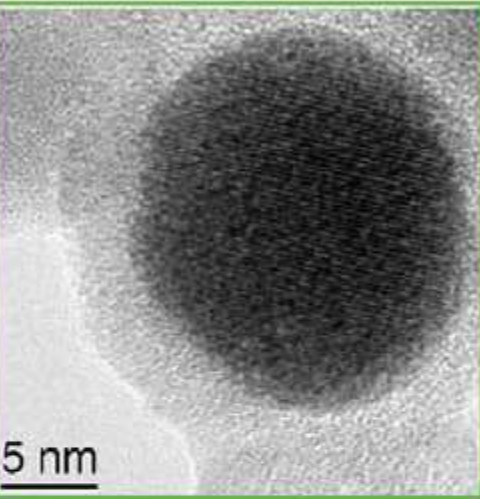
JUYOUNG KWON

- I. Introduction : nanoparticles(NPs) & magnetic nanoparticles(MNPs)
- II. Current status in clinical trials
- III. Essential requirements for fabrication of MNPs
- IV. Example of application



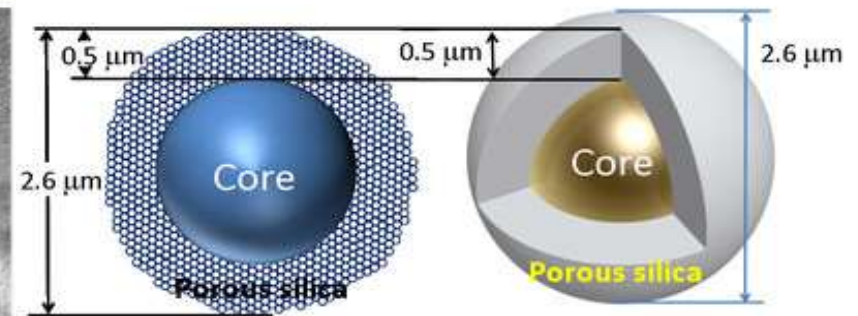
Nanoparticles (NPs)

- ✓ Made of inorganic or organic(polymeric) materials
- ✓ Characteristics different from those of bulk materials of the same composition
∴ **Size effects**
- ✓ Mainly bottom-up methods : Self-assembly



THE SOLUTION...

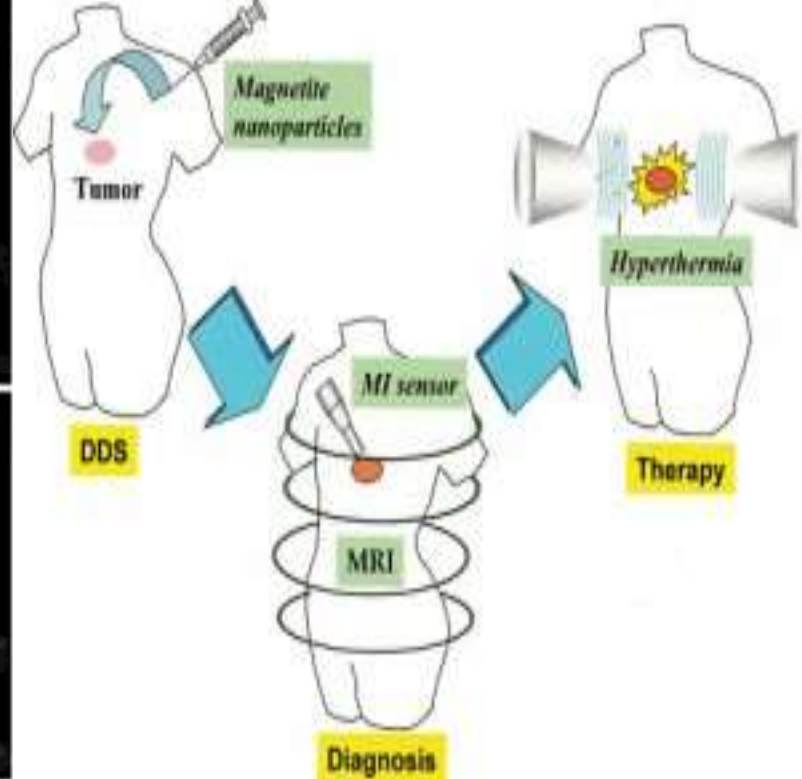
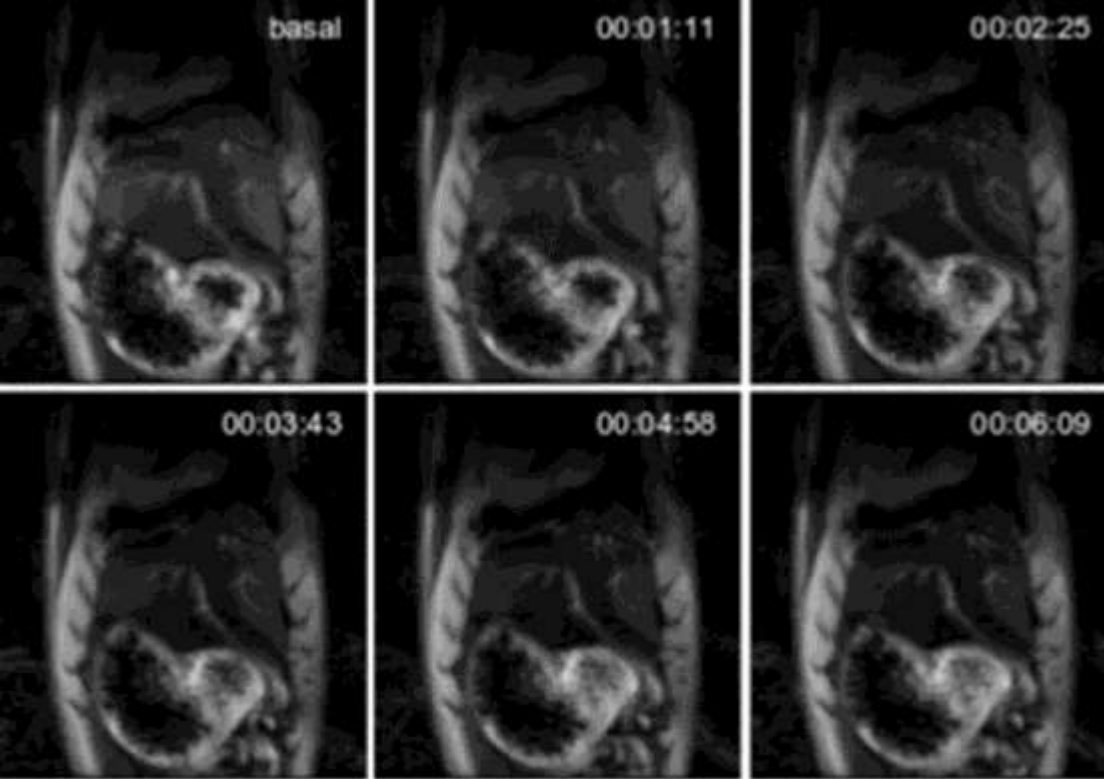
Schematic Diagram of Core Shell silica



Particle diameter: 2.6 μm , Core diameter: 1.6 μm , Thickness of porous silica: 0.5 μm
 Pore volume: 0.30mL/g, Specific surface area: 150 m^2/g , Pore diameter: 9 nm
 The ratio of porous silica volume: 77%

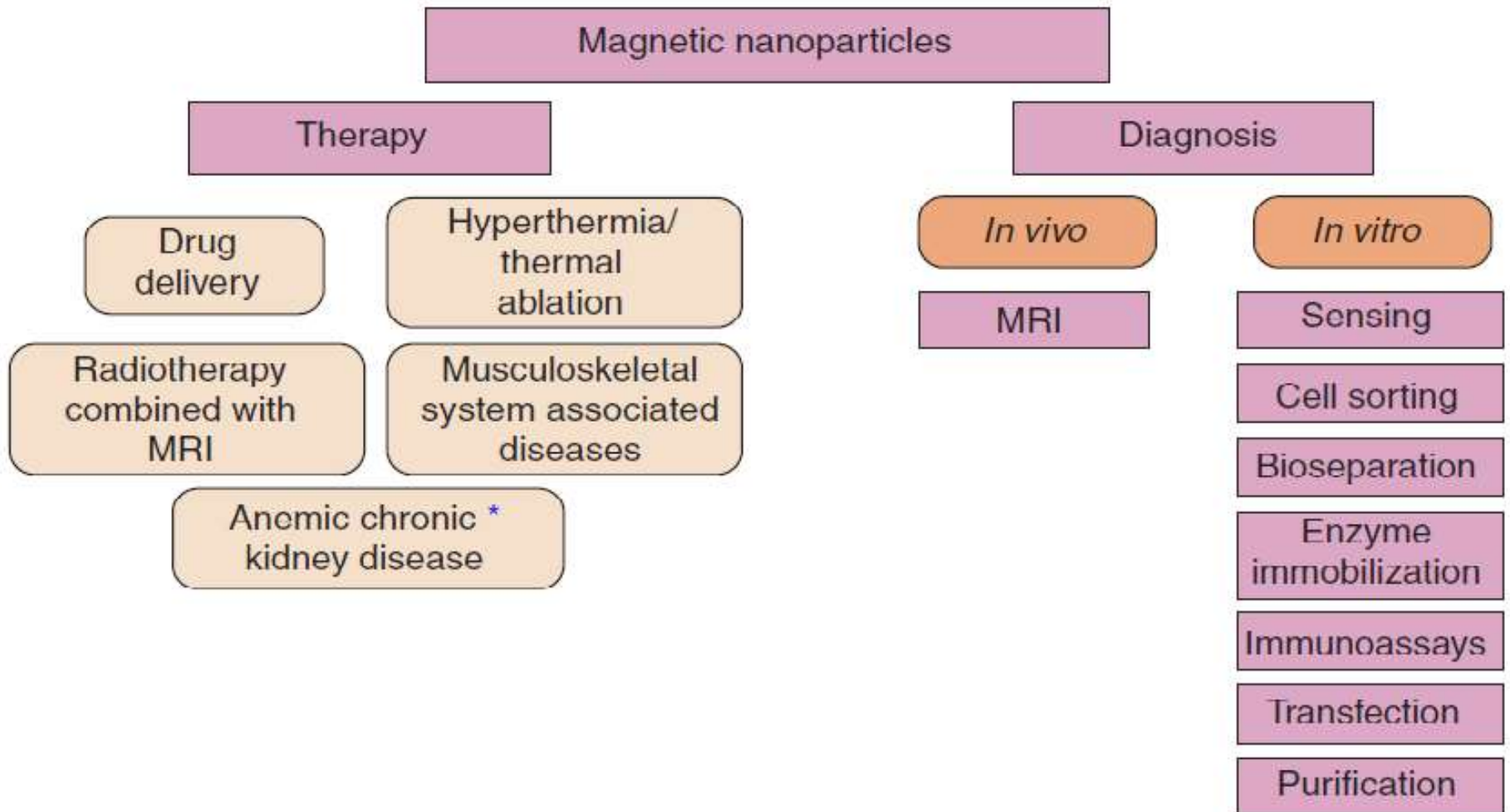
Magnetic nanoparticles (MNPs)

- ✓ Require for biomedical application
- ✓ Core-shell structure
 - **Core** : metal or metallic oxide
 - **Coating** : inorganic or polymeric materials
 - renders particles biocompatible, stable, serve as a support for biomolecules

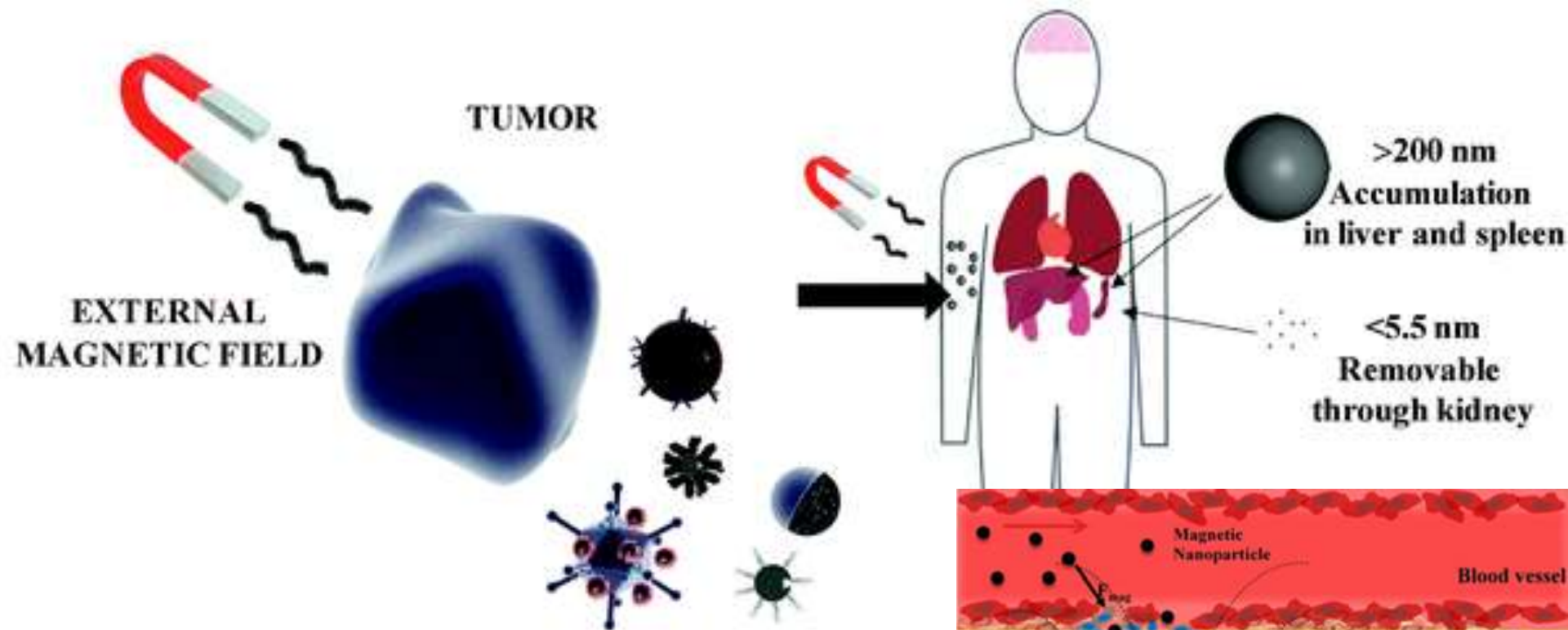


General applications of MNPs

- ✓ Magnetic contrast agents in MRI
- ✓ Hyperthermia agents
- ✓ **Magnetic vectors**
 - : directed by means of a magnetic field gradient towards a certain location, such as in the case of the targeted drug delivery



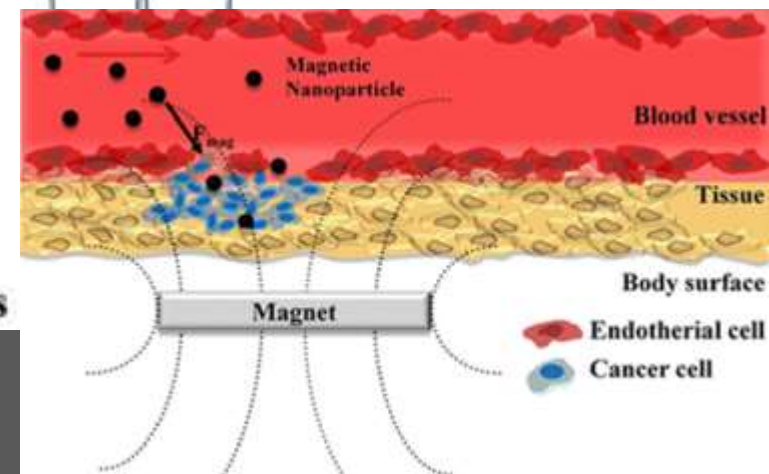
- ✓ Exploit intrinsic properties of MNPs (Biocompatibility & Selective targeting) to obtain medical breakthroughs in **diagnosis** and **drug delivery**
- ✓ Most promising applications : diagnosis and treatment of **cancer**



Specific Targeting with Magnetic Fields → 100-10 nm MNPs

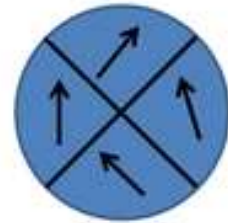
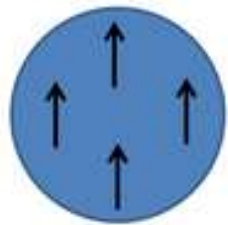
- ✓ Delivery of MNPs loaded with drug to the tumor site under the influence of external magnetic field(H_{ex})
- ✓ Only **magnetic(active)** : under the influence of H_{ex}
- ✓ Rendered **nonmagnetic(inactive)** : once H_{ex} is removed

→ Such magnetic properties acquired by very small nanoparticles (<10nm)



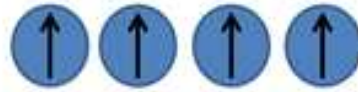
Ferromagnetic

Superparamagnetic

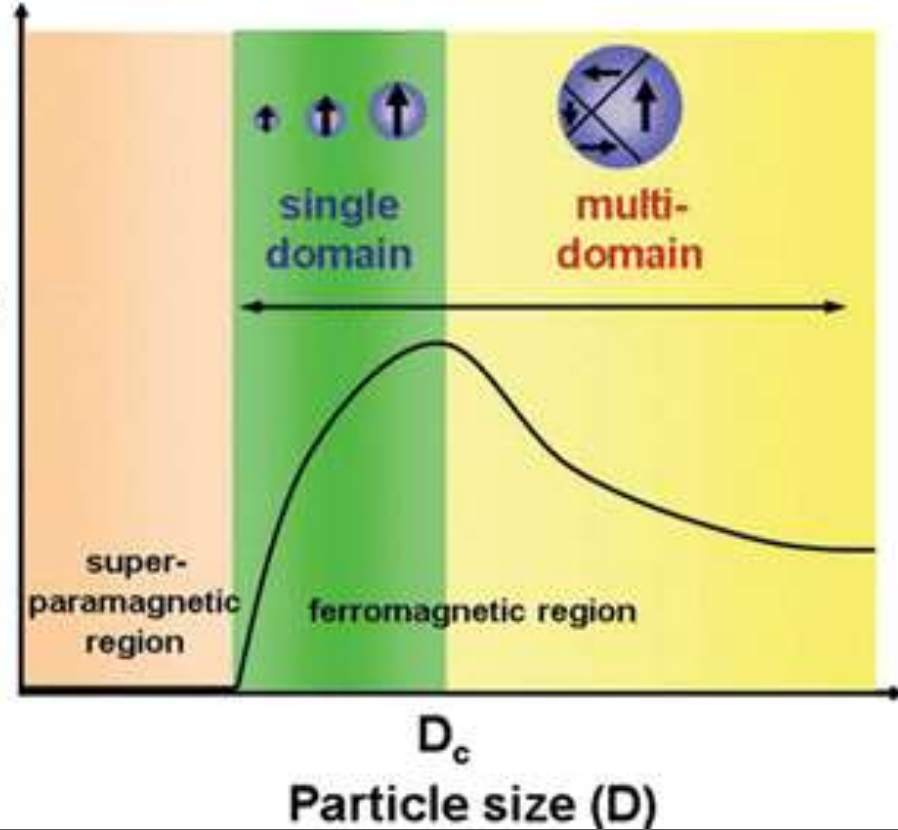


Applied
Magnetic Field

No
Magnetic Field

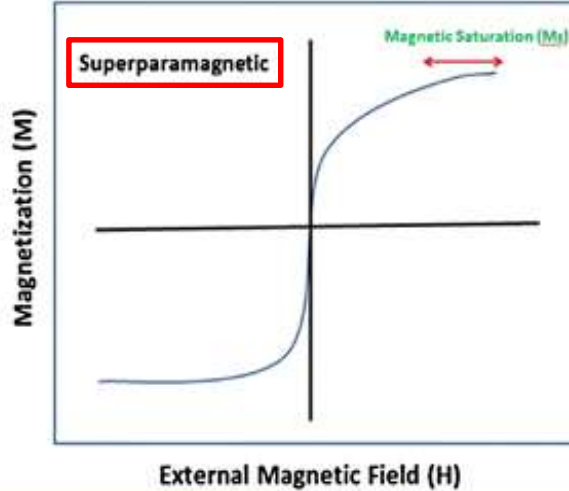


H_c

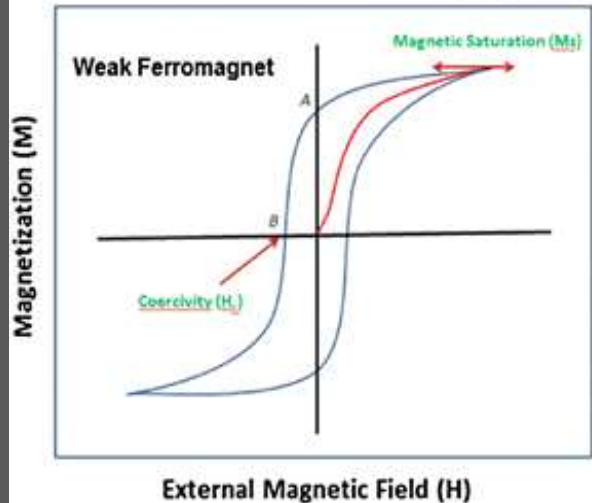


- ✓ Dimension of MNPs reduced
: $E(\text{creating domain wall}) > E(\text{supporting single-domain state})$
- ✓ Below a critical size
 - All domain walls washed away : Single-domain state
 - $H_c = 0$

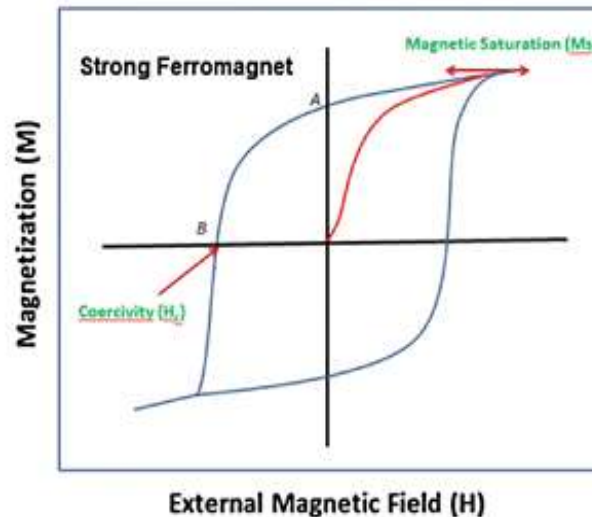
“Superparamagnetic”



External Magnetic Field (H)



External Magnetic Field (H)

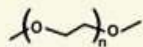


External Magnetic Field (H)

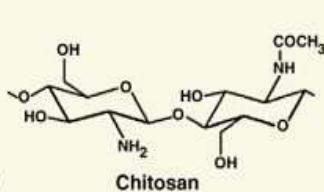
Superparamagnetic NPs

- ✓ Magnetic (in the presence of external magnet) , Nonmagnetic (removed external magnet)
- ✓ Avoid an 'active' behavior of the particles when there is no applied field
- ✓ Reverted to **nonmagnetic** states by removing Hex to allow them **to be excreted**

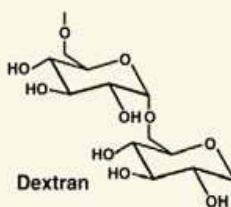
Coating Polymers



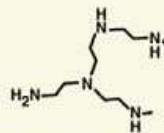
Poly(ethylene glycol) (PEG)



Chitosan



Dextran



Poly(ethylenimine) (PEI)

Polymer Types

End-grafted Polymers



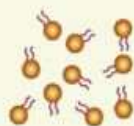
PEG

Surface Adsorption Polymers

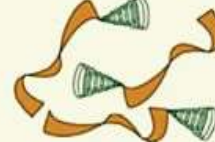


Chitosan, Dextran, PEI

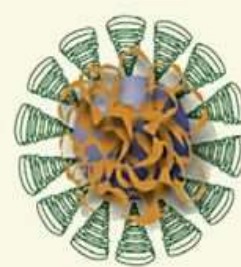
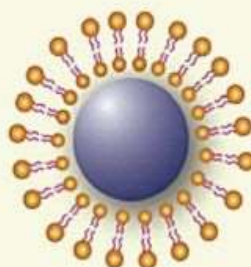
Phospholipids



CoPolymers

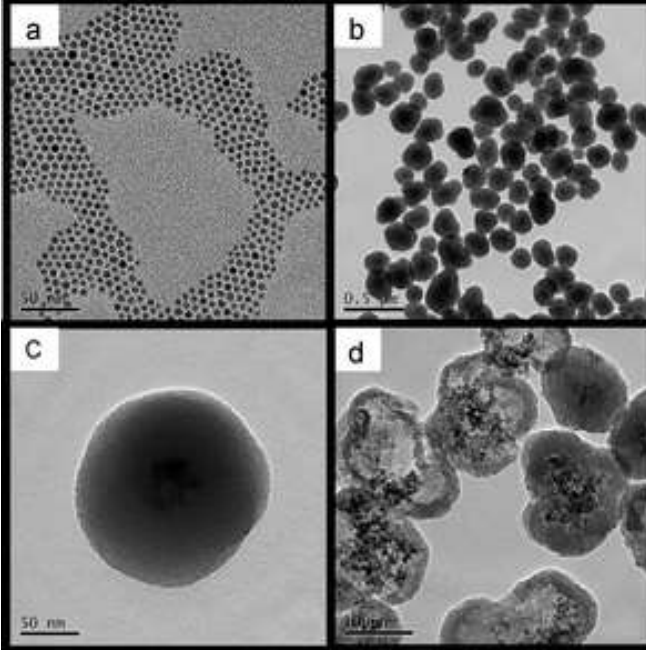
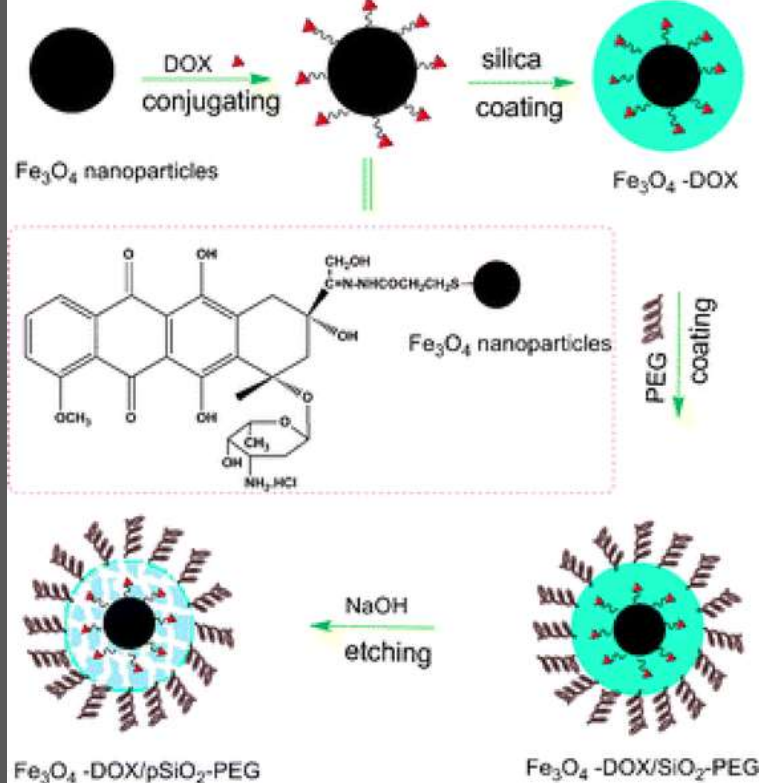


PVA-PEG, Chitosan-PEG



Surface modification

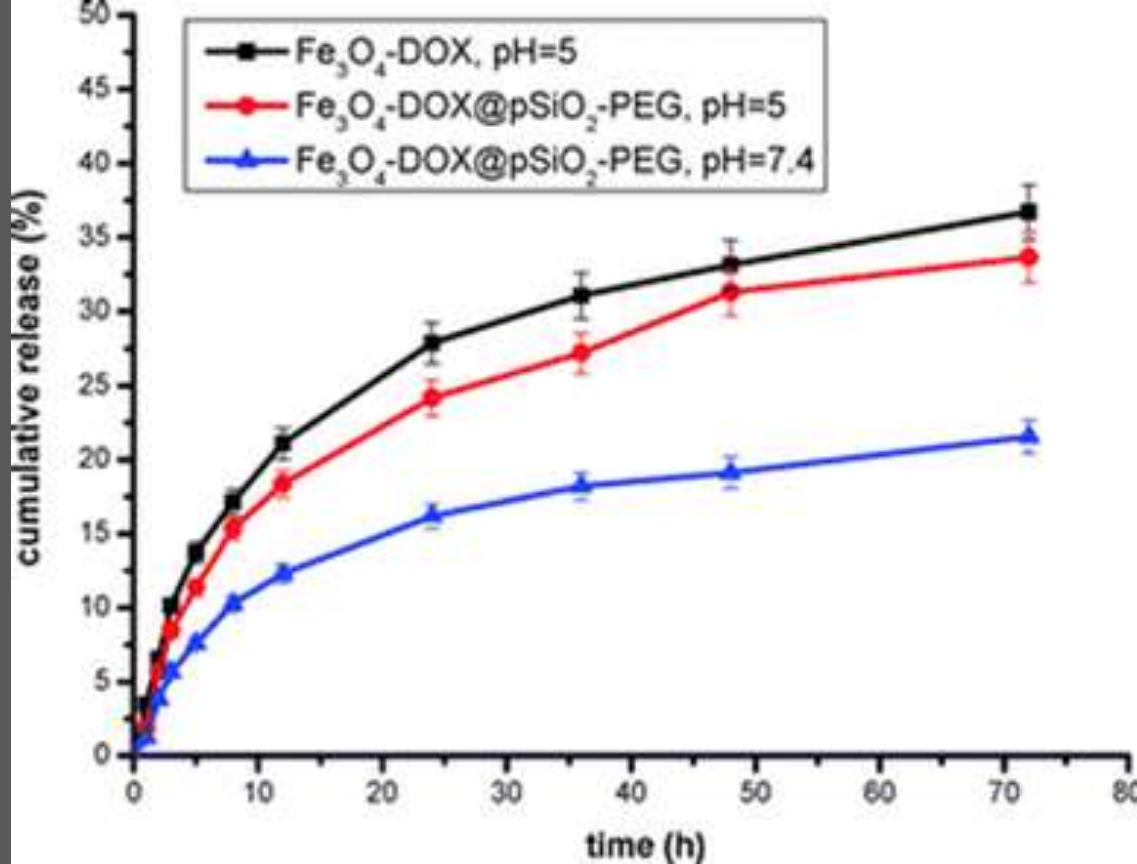
- ✓ Use of MNPs **in vivo** needs surface modification
- ✓ **To protect** from reticuloendothelial system and **increase the stability** of molecule in vivo
- ✓ Commonly used : **organic ligands** (polyethylene glycol, dextran, aminosilanes)
- ✓ Modulate the magnetic properties
 - by modifying the anisotropy
 - by decreasing the surface magnetic moment of the metal atoms located at the surface of the particles



TEM images of (a) as-prepared Fe₃O₄ nanoparticles (b, c) Fe₃O₄-DOX/SiO₂ core/shell nanoparticles (d) Fe₃O₄-DOX /pSiO₂-PEG core/shell nanoparticles

- ✓ Existing structural model
 - 1) drugs conjugated to surface of polymer coated MNPs
 - 2) Mixture of drugs & MNPs embedded in polymer

→ However, simple direct attachment of drug molecules to the surface of particles, can cause serious problems since the drug can be dissociated from the system and released in non-target areas.
- ✓ **Doxorubicin(DOX)** chemically bonded to Fe₃O₄ nanoparticles
- ✓ **Polyethylene glycol(PEG)** functionalized porous silica shell.
- ✓ **Porous silica shell**
 - Protective layer for drug molecules and magnetite nanoparticles
 - Thin barrier for the DOX release from the carrier.



- ✓ **Slower of DOX** than seen in DOX-conjugated ferrite NPs alone (because of the presence of the porous silica shell)
 - Decrease the amount of DOX dissociated from the carrier prior to release in **non-target spots** during transportation
- ✓ **Biocompatible polymer PEG** allowed to escape reticuloendothelial system, thus allowing drugs to be administered prolonged periods of time.

- ❖ Drug delivery system using MNPs provides a number of advantages in view of the carrier's therapeutic functionality
 - ✓ Good biocompatibility
 - ✓ Ease of functionalization with targeting ligands
 - ✓ High sensitivity to Hex
 - ✓ Barrier on the drug release (diffusion-control)

- ❖ Resolve primary concerns in conventional cancer therapies
 - ✓ Minimize invasive procedure
 - ✓ Reduce side effects to healthy tissues

THANK YOU